Whole-brain time-frequency analysis of event-related potentials for the assessment of pharmacodynamic effects in the human brain

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- WBTF measures change in evoked and induced event-related brain activity (ERBA)
- WBTF focuses on changes in fast sensory and later cognitive components of phase-locked even-related potentials (ERP) and not phase-locked event-related spectral perturbation (ERSP) Currently proprietary designed and recorded ERBA tasks include visual or auditory P300, MMN, CDA and N2pc.



- Selected evoked (ERP) and induced (ERSP) measures are computed on time-frequency transformed trials
- WBTF is designed to compare the whole brain differences between two conditions/sessions
 - between pre-dose baseline and post-dose tests
 - between sessions of drug treatment
 - between baseline and post-traumatic tests
- Focus on individuality; responders vs. non-responders, progression



Example of the evoked measure computed at the electrode Cz for Cond1 and Cond2 and their difference .

EEG to ERP pre-processing; re-sampling, re-referencing, filtering, artifacts processing, segmentation, baseline correction, etc.

2 Continuos Wavelet Transform (CWT); applied to each ERP trial

$$\mathit{cwt}(s, d; f(t), \Psi(t)) = \int_{-\infty}^{\infty} f(t) \frac{1}{\sqrt{s}} \Psi^*(\frac{t-d}{s}) dt$$



Picture taken from NOCIONS lab web page: http://www.nocions.org.

Morlet wavelets (*cmor1-0.5* or *cmor1-1.5*); center freq. $f_c = 0.5$ or 1.5 Hz, $f = f_c/s$



Energy normalization; to equalize |*cwt*(*s*, *d*)| mag. over scales, EEG signal at higher frequency bands has typically less power and we focus on differences over the whole time-frequency plane



Example of the energy normalization effect. Signal consisting of 2 sinusoidal waves at freq. 10 Hz and 40 Hz was transformed by CWT (cmor1-1.5)

4 Compute WBTF measures

Evoked activity measures

i) Time-frequency transformed evoked potential

$$avWT(c, f, t) = \frac{1}{N} \sum_{n}^{N} cwt(c, f, t, n)$$

ii) Inter trial phase coherence

$$ITPC(c, f, t) = \frac{1}{N} \sum_{n=1}^{N} \frac{cwt(c, f, t, n)}{|cwt(c, f, t, n)|}$$

iii) Inter trial linear coherence

$$ITLC(c, f, t) = \frac{1}{N} \sum_{n}^{N} \frac{cwt(c, f, t, n)}{\sqrt{\frac{1}{N} \sum_{n}^{N} |cwt(c, f, t, n)|^2}}$$

4 Compute WBTF measures

Induced activity measures

i) Induced power

 $Induced_{pwr}(c, f, t) = ERSP(c, f, t) - |avWT(c, f, t)|^{2}$

$$ERSP = \frac{1}{N} \sum_{n}^{N} |cwt(c, f, t, n)|^2$$

ERSP - evoked spectral perturbation

ii) Induced magnitude

$$Induced_{mag}(c, f, t) = WTav(c, f, t) - |avWT(c, f, t)|$$

$$WTav = \frac{1}{N} \sum_{n}^{N} |cwt(c, f, t, n)|$$

c-channel, f-frequency, t-time, n-trial/epoch



Example of the Induced_{DWF} (c,f,t) WBTF measure

Compute the WBTF measure differences for every time-frequency point compute a difference between Cond1 and Cond2 values of the given WBTF measure

- Baseline correction of the WBTF measure differences pre-stimulus time activities are subtracted from post-stimulus
- Cumulative difference over electrodes differences are summed over all electrodes or over selected spatial patches

8 Estimate significance of differences

Permutation testing

i) Permute Cond1 and Cond2 trials

ii) Construct permutation distribution (PD)

iii) Estimate significance of differences at each time-frequency point

iv) Correct for multiple comparisons testing

Nichols TE, Holmes AP, Nonparametric permutation tests for functional neuroimaging: a primer with examples. Human Brain Mapping, 2002 Jan;15(1):1-25.

9 Compute WBTF scores

WBTF scores

i) Significance score:
$$S_{t,f} = -\log_{10}(1 - p_{t,f})$$

 $S_{t,f} = -\log_{10}(1 - .99) = -\log_{10}(.01) = 2$

 $p_{t,f} = 0.01$ means that WBTF(t, f) is 99/100 times greater than the considered PD

ii) Total score: for each WBTF measure sum $S_{t,f}$ over all post-stimulus t, f points

iii) Composite WBTF score: combine scores by taking the maximum significance at a given *t*, *f* point over all WBTF measures



Sample of evoked sources modelling N1 and P3b event-related components



Sample of background EEG (noise) added to the pervious N1P3b model



Sample of the two induced oscillatory sources both at the level of 10nA / 40 Hz

General parameters:

- 24 electrodes following the NAS system setting
- 100 trials for each condition, sampling rate 200Hz
- time interval -200 to 900 ms, 100 ms baseline mirrored
- EEG samples were i) same or ii) different for two conditions

Evoked sources:

- 5 cortical sources modelling N1 and P3b event-related components
- three models with different amplitudes of cortical sources

Induced sources:

- 2 symmetrical induced sources at 40 Hz, sinusoidal wave with Hamming window
- four models with amplitude levels of 5, 8, 9,10 nA
- duration 300 to 450 ms, beginning randomly set 200-400 ms post-stimulus





Results for cmor1-0.5.

17/20



Results for cmor1-1.5.

18/20



Results for cmor1-0.5.

Results for cmor1-1.5.

Conclusions from analyzed simulation and clinical studies data

- Using the approach we analyze a wide collection of data from:
 - several pharmaco-clinical studies
 - traumatic brain injury (TBI) studies, diagnosing concussion and its progression
- We found that:
 - WBTF is sensitive to small evoked (ERP) and induced (ERSP) changes
 - CWT with different time-frequency resolution can be beneficial
 - Correction of multiple comparison testing should be considered
 - Statistical significance testing of the total composite and individual WBTF scores is still needed